

Application of CineECG for Enhancing Cardiac Diagnosis: Review and Cases Study.

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Abstract:

Modern cardiology relies heavily on the standard resting 12-lead Electrocardiogram (ECG), as it provides information about the electrical functionality of the heart. However, performing diagnosing using ECG depends highly on the doctor's interpretations and understanding of its complex patterns. A technique based on Vectorcardiography method called CineECG, has been developed to provide a different representation of the ECG. In this study, we reviewed the CineECG method and described the equations behind it. Additionally, we tested the method on three cases, relating to healthy, left bundle branch block, and right bundle branch block subjects to verify the CineECG utility in the diagnostic process. Our results showed easily interpretable figures that can be used to aid in the diagnosis of these cases. Thus, CineECG represents a potentially useful tool for enhancing cardiac diagnosis.

Keywords: Electrocardiography, Vectorcardiography, CineECG, Left bundle branch block, right bundle branch block.



Received:
Accepted:

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26 1. Introduction:

27 The Electrocardiogram, also known as ECG or EKG
28 (from the German "Elektrokardiographie"), is a
29 fundamental diagnostic tool in the field of
30 cardiology. It provides valuable insights into the
31 electrical activity of the heart, offering a window into
32 its health and functionality, and with the right
33 interpolation, ECG data can be used for early
34 diagnosis of many heart malfunctions, such as blood
35 clot(Thomson et al., 2019), ischemia(Wimmer et al.,
36 2013), left bundle branch block (LBBB)(Sgarbossa,
37 2000) and right bundle branch block (RBBB)(Ikeda,
38 2021) just to name a few.

39 Despite its widely use, ECG interpretation is still
40 very challenging and affected by intra- and inter-
41 subject variability. Thus, automatic algorithms for
42 the support of ECG interpretation are still desirable.

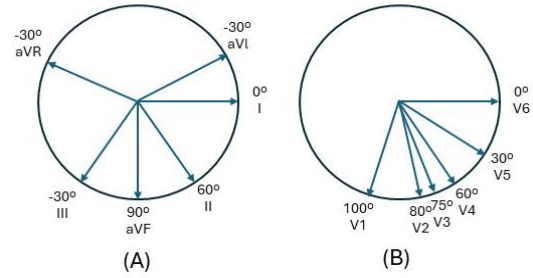
43 In this paper, we will review a novel way to look at
44 the 12-leads ECG, called CineECG, introduced in
45 2022, the method aims to describe the path of the
46 electrical activation during the heart cycle using the
47 cardiac axis, and will test the algorithm on a normal
48 case as well as clinical cases of LBBB and RBBB,
49 which are two conduction disorders that effect the
50 electrical path.

51 2. Electrocardiography and 52 Vectorcardiography:

53 Standard 12-lead ECG is the most used type of ECG,
54 it is composed of nine electrodes placed on the chest
55 and limbs of the patient. Standard 12-lead ECG
56 signals can be categorized into:

- 57 • Standard Limb Leads (I, II, III): also known as
58 Einthoven triangle, offering a frontal plane view
59 of the heart.
- 60 • Augmented Voltage Limb Leads (aVR, aVL,
61 aVF): are derived from the standard limb leads
62 and provide a view of the heart from different
63 angles in the frontal plane.
- 64 • Precordial (Chest) Leads (V1-V6): which gives
65 a transverse plane view of the heart.

66 As depicted in Figure (1), the 12 signals would
67 describe the electrical activity of the heart from
68 different angles, providing a complex understanding



69

70 Figure 1 - Standard 12-leads ECG angles, (A) limb and
71 augmented leads as seen in the frontal plane, (B)
72 precordial leads as seen in axial plane.

73 of the path of the electrical signal through the
74 structures of the heart. Because of the way it is
75 composed, a redundancy in information exists,
76 specifically in the augmented leads and the II, as
77 shown in equations 1 to 4:

$$II = I + III \quad (1)$$

$$aVL = I - \frac{II}{2} \quad (2)$$

$$aVF = II - \frac{I}{2} \quad (3)$$

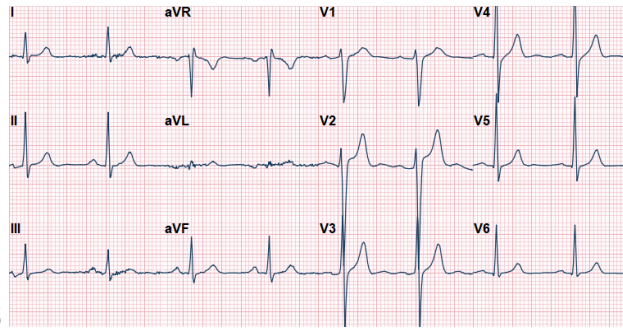
$$aVR = \frac{-(I + II)}{2} \quad (4)$$

78 While these leads aim to describe a three-
79 dimensional vector in space they are expressed as 2D
80 signals, this led to the development of
81 vectorcardiography or (VCG), a technique allows for
82 the 3D visualization of the amplitude and direction
83 of the heart activation, VCG can be calculated using
84 Franks's leads(G Daniel et al., 2007; KORS et al.,
85 1990), Equations 5 to 7.

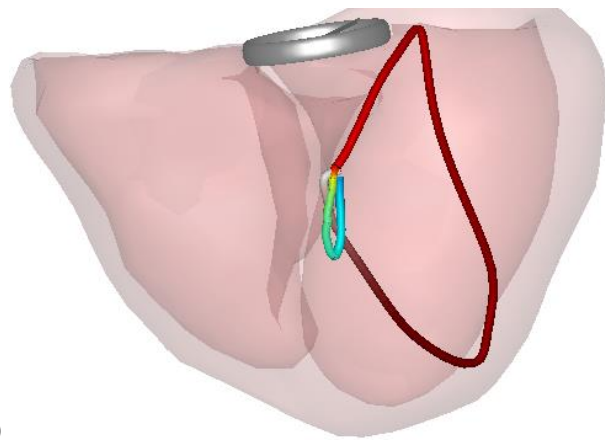
$$VCG_x = -(-0.172 V1 - 0.074 V2 + 0.122 V3 + 0.231 V4 + 0.239 V5 + 0.194 V6 + 0.156 I - 0.010 II) \quad (5)$$

$$VCG_y = (0.057 V1 - 0.019 V2 - 0.106 V3 - 0.022 V4 + 0.041 V5 + 0.048 V6 - 0.227 I + 0.887 II) \quad (6)$$

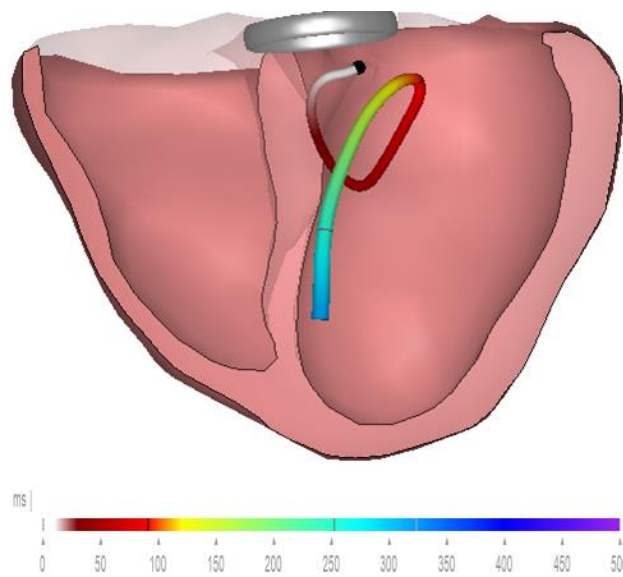
$$VCG_z = -(-0.229 V1 - 0.310 V2 - 0.246 V3 - 0.063 V4 + 0.055 V5 + 0.108 V6 + 0.022 I + 0.102 II) \quad (7)$$



86
87 Figure 2 - Standard 12 leads ECG of the control healthy
88 case.



90
91 Figure 3 - VCG for the healthy control patient.



93
94 Figure 4- CineECG of the control case.

95 Where $(VCG_x, VCG_y, \text{ and } VCG_z)$ are the vector
96 component in 3D of the VCG, I and II are the
97 reading of the first and second standard limb reads,
98 while $V1 \sim V6$ are the readings of the precordial
99 (Chest) leads. however, clinically VCG was not used
100 extensively, due to complex pattern, (ex, using the 12
101 lead ECG from healthy subject shown in Figure (2)
102 the VCG shown in Figure (3) was created, and the
103 fact that it is described using the body axis. thus, it
104 requires rotation to the heart axis.

105 Also, due the simplicity aspects of the model, *i.e.*, the
106 fixed origin vector, it cannot fit all data, which leads
107 to the loss of some information.

108 3. CineECG Methodology Review:

109 CineECG was first described here (Boonstra et al.,
110 2022), as a novel clinical way to evaluate the
111 standard 12-lead ECG by describing the average
112 location of the anatomical center of the cells that
113 undergoing a change on transmembrane potential at
114 a certain point of time, *i.e.*, the cells that are
115 simultaneously electrically activated.

116 To calculate these positions, three inputs are
117 required, that are the standard 12-lead ECG, the
118 model for the torso with the placements of the
119 electrodes and the model of the heart. In case the
120 models are not available, CineECG used generic
121 models of heart and torso.

122 CineECG considers that the average ‘velocity’ of the
123 electrical activation propagation through the heart
124 structure is 0.7 m/s. Moreover, the mid QRS
125 complex, the average position of the cardiac
126 activation is located at the center of mass of the heart,
127 and this is considered as the anchor point for the
128 CineECG, both in time and space. Once an input is
129 acquired, CineECG is calculated recursively, using
130 the following steps:

131 1. VCG is calculated using equation 8.

$$\vec{vCG} = \sum_{n=1}^9 L_n(t) a_n \left(\frac{\vec{r}_n - \vec{r}_{ref}(t)}{\|\vec{r}_n - \vec{r}_{ref}(t)\|} \right) \quad (8)$$

132 where L_n is the lead read, and a_n is a scaling factor.
133 \vec{r}_n a vector from the origin to the nth electrode, while

134 \vec{r}_{ref} is a vector from the reference point to the
 135 location of CineECG at (t-1), for t = 0, reference
 136 point is the centre of mass.

137 2. CineECG is calculated using equation 9:

$$\overrightarrow{\text{CineECG}(t)} = \overrightarrow{\text{CineECG}(t-1)} + \text{speed} \frac{\overrightarrow{\text{VCG}}}{\|\overrightarrow{\text{VCG}}\|} \quad (9)$$

138 3. Calculation is repeated backward in time.

139 The original paper(Boonstra et al., 2022) goes in
 140 depth about the calculations and all justifications for
 141 all assumptions.

142 **4. Cases analysis:**

143 Using the CineECG software shown in Figure (5), we
 144 processed 12 leads ECG data acquired from two
 145 different patients and one control healthy case, the
 146 clinical cases included: LBBB, RBBB. These cases
 147 were previously diagnosed by cardiologist. While the
 148 software can process data from multiple extensions

149 *i.e.*, (mat, ecg, pdfecg, xml, txt, inf, csv, rr, bsm, json,
 150 dcd and dcm), our data was in standard DICOM.

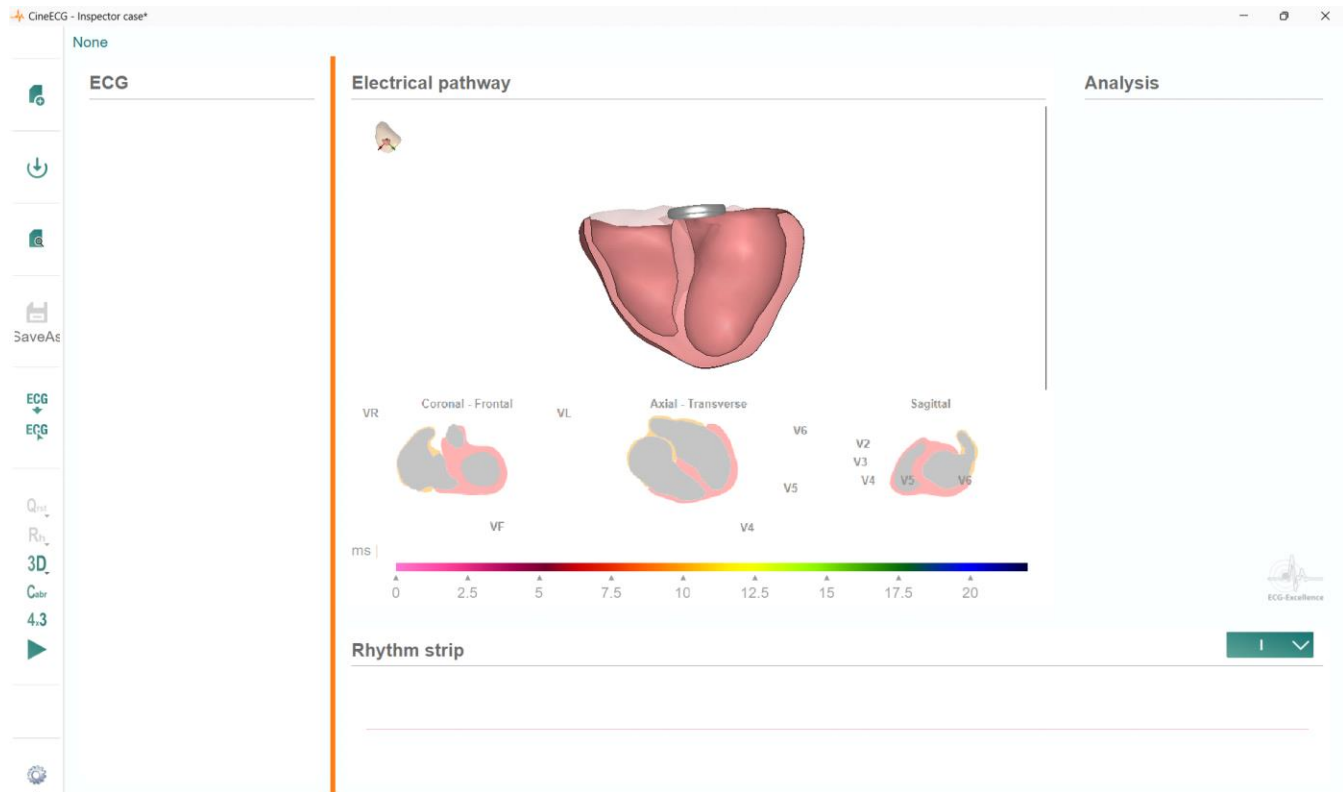
151 No preprocessing was applied outside the software as
 152 the software can perform baseline corrections and
 153 acquiring a median beat before applying the
 154 CineECG algorithm and generating the 3D visual
 155 representation.

156 **3.1. Control case:**

157 The case belongs to a healthy male with no known
 158 heart malfunctions, Figure (2) shows the standard 12-
 159 ECG in 4 by 3 format after performing the baseline
 160 correction.

161 Figure (3) shows the CineECG line generated by the
 162 software, the color gradient represents the time
 163 stamps.

164



165

166

Figure 5 - CineECG user interface, with no loaded ECG.

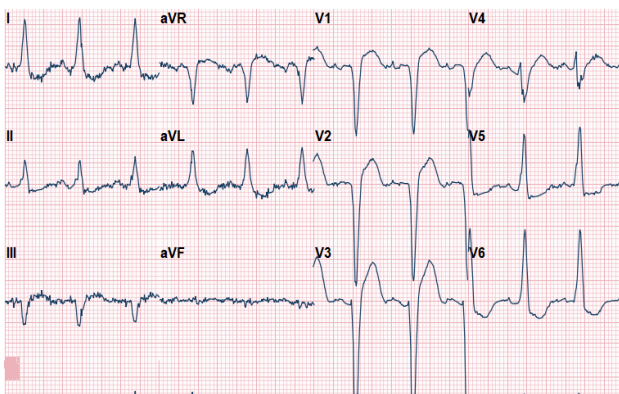
167

168 The healthy case can be described in three phases.

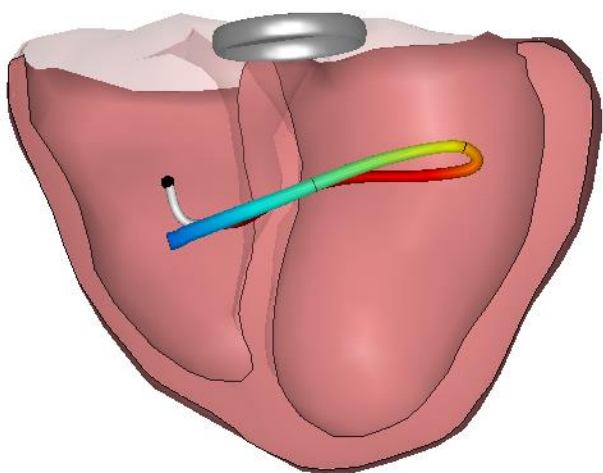
- 169 a) QRS complex: the line propagates through the
- 170 septum, followed by the line moving toward
- 171 the apex and the left free wall, before making a
- 172 turn towards the base around the R top.
- 173 b) ST segment: the vector is propagating towards
- 174 the apex, with shifting to the interior and the
- 175 septum.
- 176 c) T-wave: the line shows moving toward the
- 177 apex.

178
179 **3.2. LBBB case:**

180 Figure (6) shows the standard 12-leads of an LBBB
181 patient, after baseline correction, and Figure (7)
182 shows the generated CineECG. The electrical path
183 in the CineECG clearly differs from the normal
184 case,



185
186 Figure 6- CineECG of the LBBB case.



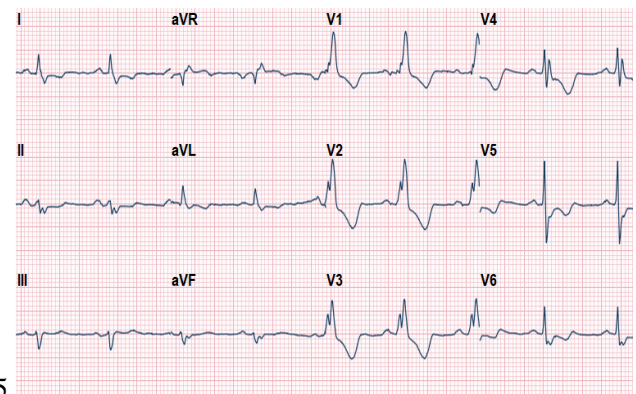
187
188 Figure 7 - CineECG of LBBB case.

189 and with further inspections we can see it starts
190 from the right ventricle, travel through the septum
191 to the left ventricle, and for the repolarization is
192 traveling from the left ventricle to the right one.

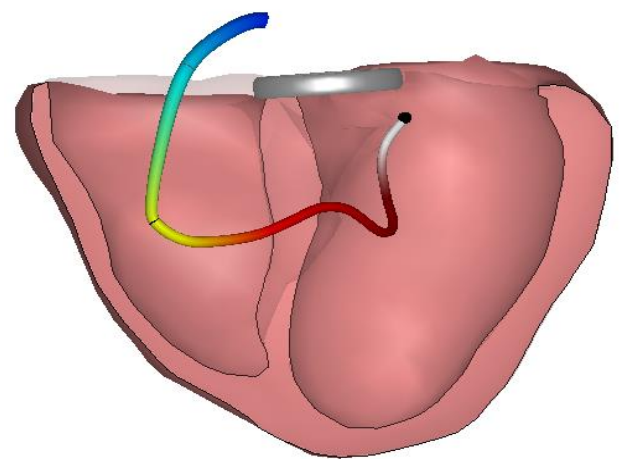
193 **3.3. RBBB Case:**

194 Figure (8) shows the standard 12-leads ECG of an
195 RBBB patient, after baseline correction while the
196 CineECG is shown in Figure (9). Just like in LBBB
197 case the CineECG line shows different from the
198 normal path. In the case of RBBB, the CineECG
199 line starts from the left ventricle followed by
200 moving towards the right one through the septum,
201 and then the repolarization line is traveling toward
202 the base instead of the apex.

203
204



205
206 Figure 8 - Standard 12-lead ECG of the RBBB.



207
208 Figure 9- CineECG in case of RBBB.

209

210 5. Discussion:

211 The aim of the present work was to review the
212 software CineECG, in order to demonstrate its
213 innovative ability in supporting the clinicians in the
214 standard 12-lead interpretation.

215 The control case findings agree with what we
216 already know about the path of the electrical signal
217 in the heart starting from the Atrioventricular (AV)
218 Node, then down using the bundle of His, then to
219 the left and right ventricles using the bundle
220 branches with the line shifted toward the left
221 ventricle because of its bigger mass comparing to
222 the right, finally although the Repolarization travel
223 from the apex to the base, the charge is reversed
224 and thus it shows raveling towards the apex. This
225 case showed a true potential for the tool as well as
226 established a reference to be considered when
227 examining the clinical cases.

228 LBBB and RBBB are diagnosed primarily by ECG
229 where the electrical activity in the LBBB ECG
230 shows symptoms like widened QRS complex (>
231 120 ms), a dominant S wave in lead V1, broad,
232 monophasic R wave in lateral leads (I, aVL, V5-
233 V6), and an absence of Q waves in lateral
234 leads (Nikoo et al., 2013). While the RBBB, shows
235 morphologies like a widened QRS complex (> 120
236 ms), what is known as RSR' pattern in leads V1-V3
237 (appearing like an "M") and a wide, slurred S wave
238 in lateral leads (I, aVL, V5-V6) (Surawicz et al.,
239 2009). These finding are not easy to recognise, as
240 it may differentiate among patients, and it requires
241 much expertise and understanding of the ECG to
242 be diagnosed.

243 However using the CineECG for the LBBB case,
244 the visual indicate a problem with the signal path
245 moving toward the left ventricle since the right
246 ventricle is activated before it, which agree with the
247 diagnosis of the LBBB.

248 And for the RBBB case the observations agree as
249 well with the block in the right bundle which
250 causes the delay in the depolarization and given the
251 fact the T-wave is reversed in this case of RBBB,
252 that explain the inverse direction of the
253 repolarization wave.

254 These cases showed the fact that the algorithm can
255 give a good representation of the 12-Lead ECG, a
256 representation that can be used as a diagnostic tool

257 as well as an informatic educational tool as it
258 describes the 12 signals with a single line./

259 Limitations do exist in terms of using the generic
260 heart and torso model, in some cases this could
261 generate non accurate data, however, with the
262 evaluation of auto image segmentation methods
263 specifically the deep learning-based methods, this
264 problem could be dealt with. In the future we look
265 forward to quantifying these visual observations to
266 provide better understanding and explore the
267 ability to automate the diagnosis procedure. An
268 educational demonstration version of CineECG,
269 can be downloaded for free at
270 <https://cineecg.com/free-trial>.

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